## Short communication

# Fabrication and characterization of hydrophobic microarc oxidation/ poly-lactic acid duplex coating on biodegradable $\mathrm{Mg}-\mathrm{Ca}$ alloy for corrosion protection 

H.R. Bakhsheshi-Rad ${ }^{\text {a, b, * }}$, E. Hamzah ${ }^{\text {a }}$, R. Ebrahimi-Kahrizsangi ${ }^{\text {b }}$, M. Daroonparvar ${ }^{\text {a }}$, M. Medraj ${ }^{\mathrm{c}, \mathrm{d}}$<br>${ }^{\text {a }}$ Department of Materials, Manufacturing and Industrial Engineering, Faculty of Mechanical Engineering, Universiti, Teknologi Malaysia, 81310 Johor Bahru, Johor, Malaysia<br>${ }^{\text {b }}$ Advanced Materials Research Center, Materials Engineering Department, Najafabad Branch, Islamic Azad University, Najafabad, Iran<br>${ }^{\text {c }}$ Department of Mechanical Engineering, Concordia University, 1455 De Maisonneuve Blvd.West, Montreal, QC H3G 1M8, Canada<br>${ }^{\text {d }}$ Mechanical and Materials Engineering, Masdar Institute, Masdar City, P.O. Box 54224, Abu Dhabi, United Arab Emirates

## A R T I C L E I N F O

## Article history:

Received 17 December 2015
Accepted 29 December 2015
Available online 2 January 2016

## Keywords:

Mg-Ca alloy
Microarc oxidation
Hydrophobic properties
Bio-corrosion behavior


#### Abstract

A double layer coating was prepared on biodegradable $\mathrm{Mg}-\mathrm{Ca}$ alloy by microarc oxidation (MAO) followed by dip coating process. The results showed that hydrophobic poly-lactic acid (PLA) as a top layer with thickness of $37-40 \mu \mathrm{~m}$ provides significantly higher corrosion resistance in terms of corrosion current and charge transfer resistance, while the MAO coating alone ( $8-10 \mu \mathrm{~m}$ ) exhibits lower corrosion resistance. However, both coating scenarios demonstrate better corrosion resistance compared with the uncoated Mg-1.34wt\% Ca alloy. Contact angle (CA) measurements showed that the double layer MAO/ PLA coated sample presented hydrophobic properties with a CA of $95.30^{\circ}$ which is higher than that of MAO coating $\left(C A=22.90^{\circ}\right)$. The results also exhibit that hydrophobic PLA is effectively seals the porosities of the MAO layer providing effective protection for the biodegradable Mg alloy in the simulated body fluid (SBF) environment and improving the corrosion protection capacity of the MAO surface treatment.


© 2016 Elsevier Ltd. All rights reserved.

Biomedical applications (such as orthopedic, cardiovascular and tissue engineering) of magnesium and its alloys are hindered by their poor corrosion resistance compared to other metals such as titanium alloys, cobalt chromium alloys and stainless steels [1]. Coatings are considered as an effective method to enhance the poor corrosion resistance and to control the degradation rate of Mg alloys in physiological environments. Typical surface modification techniques include electrodeposition (ED), physical vapour deposition (PVD) [2], laser cladding, dip coating [2], ion implantation [3] and chemical conversion coatings [4]. Micro-arc oxidation (MAO) is a chemical conversion process and is one of the most appropriate method for Mg alloys owing to its excellent abrasive resistance, enhanced corrosion resistance and high bonding strength to the

[^0]substrate [3,5-7]. However, MAO coating is not able to provide long term corrosion protection for Mg alloys in physiological environment owing to its porous structure [5,8]. Therefore, polymer coating have been employed to seal the pores of the MAO coating on the surface of Mg alloys [3]. In this view, dip coating which is a suitable and relatively simple technique is used in this work for applying the poly-lactic acid (PLA) coating as an overlayer to seal the pores and cracks of the MAO layer and to prevent its premature failure. PLA is a naturally biodegradable material with biological properties suitable for the production of bioabsorbable orthopedic implants and micro-devices for intravenous controlled release of drugs [9,10]. Thus, in the present study, a combination of MAO and PLA polymer coating was applied to provide a double-layer coating in order to improve the coating adhesion to the substrate and to enhance the corrosion resistance of the $\mathrm{Mg}-\mathrm{Ca}$ alloy in physiological conditions. Therefore, samples of $\mathrm{Mg}-1.34 \mathrm{wt}$ \% Ca alloy with dimensions of $15 \mathrm{~mm} \times 10 \mathrm{~mm} \times 10 \mathrm{~mm}$ were used as substrates. For MAO coating, a sodium aluminate-based aqueous solution consisted of $3 \mathrm{~g} / \mathrm{L} \mathrm{KF}$ and $10 \mathrm{~g} / \mathrm{L} \mathrm{NaAlO} 2$ was employed as an
electrolyte. A flat stainless-steel plate and the Mg-1.34Ca alloy sample were used as a counter electrode and working electrode, respectively. MAO was performed at a constant current density of 5 $\mathrm{A} / \mathrm{cm}^{2}$ at $15^{\circ} \mathrm{C}$ for 60 min using a DC pulse power supply and a stirring and cooling systems. A pulse frequency was fixed at 100 Hz and the duty cycle (the ratio between pulse width and pulse repetition time) was $6 \%$. Prior to the dipping of MAO coated sample, $6 \mathrm{wt} . \%$ PLA pellets ( $M_{\mathrm{w}}=148,000 \mathrm{~g} / \mathrm{mol}$, Minneapolis, MN) were dissolved in dichloromethane (DCM; $\mathrm{CH}_{2} \mathrm{Cl}_{2}$, Sigma-Aldrich, UK) by stirring for 2 h at room temperature. The samples were dipped for 3 times and withdrawn at a constant speed of $40 \mathrm{~mm} / \mathrm{min}$ to form a uniform coating and then dried at room temperature. X-ray diffractometry (Siemens-D500) was used for phase identification using $\mathrm{Cu}-\mathrm{K} \alpha$ radiation generated at 40 kV and 35 mA . Microstructural observation was performed using a scanning electron microscope (SEM; JEOL JSM-6380LA). The details of the bonding strength tests and bio-corrosion experiments can be found in our previous paper [11]. A three-electrode cell was used for potentiodynamic polarization (PARSTAT 2263) and electrochemical impedance spectroscopy (EIS) tests in simulated body fluid (SBF) solution according to [11]. The SEM micrographs and EDX analysis in (Fig. 1a,d) show the presence of a eutectic lamellar structure composed of $\mathrm{Mg}_{2} \mathrm{Ca}$ and $\alpha-\mathrm{Mg}$ at the grain boundaries of the $\mathrm{Mg}-\mathrm{Ca}$ alloy which is consistent with the $\mathrm{Mg}-\mathrm{Ca}$ phase diagram [12]. The microstructure of the MAO coating is presented in Fig. 1b,e and shows a great amount of porosity and micro-cracks resulting in a rough surface. Formation of such porosity is attributed to the sparking discharge and gas bubbles at the surface of the anode. While crack formation can be related to the thermal stresses resulting from the rapid re-solidification of the molten surface oxide [13]. These pores and micro cracks adsorb corrosion species which deems the coating not very resistant to corrosion. However, after PLA polymer coating, the porous structure of the MAO layer is sealed with a uniform polymeric layer (Fig. 1c,d) to improve the corrosion resistance of the MAO coating. The EDS analysis of the MAO coating showed that it is porous and contains $\mathrm{Al}, \mathrm{Na}, \mathrm{Si}, \mathrm{O}$, and Mg . The high intensity Al element comes from the electrolyte, It reacts with Mg and O to form the $\mathrm{MgAl}_{2} \mathrm{O}_{4}$ (spinel) porous outer layer. The EDS analysis of the PLA overlayer showed the presence of C and O .

Cross section microstructure shows that the thickness of MAO coating is around $8-10 \mu \mathrm{~m}$. This coating was bonded with the $\mathrm{Mg}-\mathrm{Ca}$ alloy via sintered interlocking. The MAO layer indicated a
bi-layered structure which is consisted of an outer porous layer and a dense inner layer (Fig. 2a). This peculiar structure is a result of the fact that the oxide grows in the MAO treatment in both inwards and outwards directions from the original Mg alloy surface. There is a good agreement between this finding and typical structure of the MAO coatings [13]. In MAO/PLA coating, two-layer structure can be observed which contains a PLA layer with a thickness of $30-35 \mu \mathrm{~m}$ as the top layer and MAO layer as the underlayer (Fig. 2b). It is also obvious that the PLA uniformly covers and seals the surface of the MAO coating. In this regard, there is a good adhesion between the substrate/coating and no obvious micro-cracks could be detected at the interface of MAO/PLA. The results of bonding strength tests showed that the mono MAO layer presented good bonding strength ( 23.5 MPa ), while, the MAO/PLA coating exhibited lower bonding strength ( 14.7 MPa ). However, compared to the direct PLA coating on the surface of Mg alloy, i.e. without MAO treatment, that had a bonding strength of 2.5 MPa only [14], the bi-layer MAO/PLA coating demonstrated significantly higher bonding strength. This is because the intermediate MAO layer provides good bonding through mechanical interlocking effect.

The XRD patterns of the uncoated sample confirms the SEM/EDS microstructural observations regarding the formation of the $\mathrm{Mg}_{2} \mathrm{Ca}$ compound besides $\alpha$-Mg (Fig. 3a) which is in agreement with the $\mathrm{Mg}-\mathrm{Ca}$ phase diagram [12]. The pattern of the MAO coated $\mathrm{Mg}-\mathrm{Ca}$ alloy depicts that this layer consists of MgO and $\mathrm{MgAl}_{2} \mathrm{O}_{4}$ phases along with $\alpha-\mathrm{Mg}$. The presence of $\alpha-\mathrm{Mg}$ peaks in the MAO XRD pattern is due to the porous structure of the MAO layer resulting in the X-rays reaching the Mg alloy surface. However, the presence of $\mathrm{MgAl}_{2} \mathrm{O}_{4}$ is attributed to the presence of aluminate ions ( $\mathrm{AlO}^{2-}$ or $\mathrm{Al}_{2} \mathrm{O}_{4}^{2-}$ ) in the electrolyte which react with $\mathrm{Mg}^{2+}$ ions at the oxide/ electrolyte interface, leading to the formation of $\mathrm{MgAl}_{2} \mathrm{O}_{4}$ [15]. The duplex coating MAO/PLA samples consist of two intense peaks at $2 \theta=16.68^{\circ}$ and $2 \theta=18.96^{\circ}$ which is in agreement with the results of Sacchetin et al. [9]. The contact angle of the uncoated and coated samples showed that the uncoated $\mathrm{Mg}-\mathrm{Ca}$ sample has a hydrophilic surface with contact angle (CA) of $42.30^{\circ}$ (Fig. 3b). However, MAO coating is even more hydrophilic ( $\mathrm{CA}=22.90^{\circ}$ ), as the water droplet easily wets and spreads out over the MAO film and quickly penetrate into the sample. In contrast, the double layer MAO/PLA coated sample presents hydrophobic properties with a CA of $95.30^{\circ}$, indicating that the polymer coating over MAO layer can effectively diminish its contact area with the corrosive aqueous


Fig. 1. Surface morphology of (a,d) uncoated $\mathrm{Mg}-\mathrm{Ca}$ alloy, (b,e) mono-layer MAO coating and (c,f) bi-layer MAO/PLA coating.


Fig. 2. Cross sectional SEM micrographs of (a) mono-layer MAO coating and (b) bi-layer MAO/PLA coating.


Fig. 3. (a) X-ray diffraction patterns and (b) Images of water contact angle of uncoated, MAO coating and MAO/PLA coating Mg-Ca alloy.
solution, which would result in significant improvement in corrosion resistance.

The electrochemical polarization curves in Fig. 4a show that the corrosion potential ( $\mathrm{E}_{\text {corr }}$ ) of the MAO/PLA coated $\mathrm{Mg}-\mathrm{Ca}$ alloy is -1530 mV SCE which is approximately 256 mV SCE higher than that of the uncoated sample ( $-1786 \mathrm{mV}_{\text {SCE }}$ ). It is also found that the $\mathrm{E}_{\text {corr }}$ of the MAO coated $\mathrm{Mg}-\mathrm{Ca}$ alloy is -1576 mV SCE , indicating that both coated samples have more positive $\mathrm{E}_{\text {corr }}$ than that of the uncoated samples. In addition, a significant decrease in the $i_{\text {corr }}$ to $7.3 \mu \mathrm{~A} / \mathrm{cm}^{2}$ from $241.5 \mu \mathrm{~A} / \mathrm{cm}^{2}$ was observed after the MAO coating. The presence of non-interconnected micro-defects in the relatively thick MAO layer can slow the transportation of the electrolyte and reduce $i_{\text {corr }}$ of the coated sample [16,17]. Note that MAO/PLA coating underwent lowest $i_{\text {corr }}$ of $0.03 \mu \mathrm{~A} / \mathrm{cm}^{2}$ which can be attributed to the sealing of porosities and microcracks of the MAO coating and thus interrupting the penetration of the corrosive species to the Mg substrate.

The EIS spectra of uncoated and coated samples demonstrated capacitive depressed semicircles in the high frequency region (Fig. 4b). After single layer and double layer coating, the capacitive loop of uncoated Mg alloy is evidently enlarged, indicating that the corrosion resistance is extremely increased. The EIS spectra of uncoated and coated samples can be fitted well using a simple equivalent circuit to characterize the samples (Fig. 4b) where $R_{e}$ represents the solution resistance, $\mathrm{C}_{\mathrm{c}}$ is the coating capacitance and
$\mathrm{R}_{\mathrm{ct}}$ is the charge transfer resistance. As can be observed in the graph the charge transfer resistance ( $\mathrm{R}_{\mathrm{ct}}$ ) of uncoated, MAO and MAO/PLA coating were $1.49,6.58$ and $2591.3 \mathrm{k} \Omega \mathrm{cm}^{2}$ respectively, indicating difficulty in charge transfer and good corrosion protection ability of the double-layer coated sample. The polarization test and EIS study revealed that a high level of corrosion protection of the Mg substrate can be provided by MAO/PLA coating through sealing of the MAO porosities and blocking the ionic transport in the MAO coating, including, e.g., chloride ion penetration through pores and subsequently the formation of a galvanic cell $[13,16,18]$. Based on these observations, the following mechanism is proposed to elucidate the corrosion process. First, when the electrolyte reaches the MAO coating/Mg alloy interface via pores in the coating, the corrosion starts by forming magnesium hydroxide at the interface, accompanied with its dissolution and re-formation at the freshly exposed surface (Fig. 4c). Replacing $\mathrm{OH}^{-}$by $\mathrm{Cl}^{-}$leads to the formation of more soluble magnesium chloride compound, which results in locallized dissolution of the surface film and exposing bare surface to re-attack [12]. Next, the Mg alloy begins to dissolve accompanied with hydrogen evolution. Hydrogen exerts pressure on the MAO coating causing forming cracks and rupture [19-21]. However, after PLA coating, the surface of the MAO layer is homogenously covered, thus transportation of corrosive ions ( $\mathrm{Cl}^{-}$) and electrolyte was largely hindered. Therefore, it can be stated that the MAO/PLA double-layer coating provides reasonable corrosion


Fig. 4. (a) Potentiodynamic polarization curves, (b) Electrochemical impedance spectroscopy measurements and (c) Schematic illustration of electrochemical corrosion mechanism of MAO/PLA coating in the SBF solution.
barrier for the $\mathrm{Mg}-\mathrm{Ca}$ alloy in the SBF environment. However, upon increasing the immersion time, it is expected that corrosive species will reach the interface with Mg alloy and hydrogen gas will be released that may cause bursting or delamination of the coating layer.

The results of the present study show that a PLA layer can be prepared on a MAO-coated $\mathrm{Mg}-\mathrm{Ca}$ alloy via relatively simple method. This results in significant increase in contact angle from $42.30^{\circ}$, for the uncoated alloy to $95.30^{\circ}$ for the duplex coating. The adhesive strength of MAO/PLA coating is 14.7 MPa which is lower compared to the MAO coating ( 23.4 MPa ). In comparison with the single layer MAO coating, the double layer MAO/PLA coating demonstrates considerably lower corrosion current density ( $0.03 \mu \mathrm{~A} / \mathrm{cm}^{2}$ ) and higher charge transfer resistance (2591.3 $\mathrm{k} \Omega \mathrm{cm}^{2}$ ). The results also exhibit that sealing the porous MAO layer by PLA polymer coating considerably enhances the corrosion resistance of the Mg alloy in the SBF physiological environment and demonstrates the potential of the MAO treatment for biomedical applications.

## Acknowledgments

The authors would like to thank the Malaysian Ministry of Higher Education (MOHE) and Universiti Teknologi Malaysia for providing the financial support and facilities for this research.
M.V. Sidorova, A.S. Gnedenkov, Corros. Sci. 85 (2014) 52-59.
[2] H.R. Bakhsheshi-Rad, E. Hamzah, M.R. Abdul-Kadir, M. Daroonparvar, M. Medraj, Vacuum 119 (2015) 95-98.
[3] X. Lin, L. Tan, Q. Zhang, et al., Acta Biomater. 9 (2013) 8631-8642.
[4] G.E. Jai Poinern, S. Brundavanam, D. Fawcett, Am. J. Biomed. Eng. 2 (2012) 218-240.
[5] S.V. Gnedenkov, S.L. Sinebryukhov, D.V. Mashtalyar, I.M. Imshinetskiy, A.S. Gnedenkov, A.V. Samokhin, Y.V. Tsvetkov, Vacuum 120 (2015) 107-114.
[6] S. Sarbishei, M.A.F. Sani, M.R. Mohammadi, Vacuum 108 (2014) 12-19.
[7] S. Dejiu, C. Jingrui, L. Guolong, H. Donglei, W. Lailei, M. Haojie, X. Yonghong, C. He, Y. Yaqian, Vacuum 99 (2014) 143-148.
[8] L. Wen, Y. Wang, Y. Zhou, L. Guo, J.-H. Ouyang, Corros Sci. 53 (2011) 473-480.
[9] P.S.C. Sacchetin, R.F. Setti, P.d.T.V.e. Rosa, Â.M. Moraes, Mater. Sci. Eng. C 58 (2016) 870-881.
[10] X. Li, C.L. Chu, L. Liu, X.K. Liu, J. Bai, C. Guo, F. Xue, P.H. Lin, P.K. Chu, Biomaterials 49 (2015) 135-144.
[11] H.R. Bakhsheshi-Rad, E. Hamzah, M. Daroonparvar, S.N. Saud, M.R.A. Kadir, Vacuum 110 (2014) 127-135.
[12] M. Mezbahul-Islam, A.O. Mostafa, M. Medraj, J. Mater. 2014 (2014) 33.
[13] L. Zhang, J. Zhang, C.-f Chen, Y. Gu, Corros. Sci. 91 (2015) 7-28.
[14] L. Xu, A. Yamamoto, Colloids Surf. B Biointerfaces 93 (2012) 67-74.
[15] L. Chang, L. Tian, W. Liu, X. Duan, Corros. Sci. 72 (2013) 118-124.
[16] X.-j. Cui, X.-z. Lin, C.-h. Liu, R.-s. Yang, X.-w. Zheng, M. Gong, Corros. Sci. 90 (2015) 402-412.
[17] J. Qian, Y. Yin, T. Li, X. Hu, C. Wang, S. Li, Vacuum 117 (2015) 55-59.
[18] M.A. Surmeneva, R.A. Surmenev, Vacuum 117 (2015) 60-62.
[19] M. Daroonparvar, M.A.M. Yajid, H.R. Bakhsheshi-Rad, N.M. Yusof, et al., Vacuum 108 (2014) 61-65.
[20] M. Daroonparvar, M.A.M. Yajid, N.M. Yusof, H.R. Bakhsheshi-Rad, E. Hamzah, Ceram. Int. 42 (2016) 357-371.
[21] H.R. Bakhsheshi-Rad, E. Hamzah, M. Kasiri-Asgarani, et al., Mater. Sci. Eng. C 60 (2016) 526-537.

## References

[1] S.V. Gnedenkov, S.L. Sinebryukhov, D.V. Mashtalyar, V.S. Egorkin,


[^0]:    * Corresponding author. Department of Materials, Manufacturing and Industrial Engineering, Faculty of Mechanical Engineering, Universiti, Teknologi Malaysia, 81310 Johor Bahru, Johor, Malaysia.

    E-mail addresses: rezabakhsheshi@gmail.com, bhamidreza2@live.utm.my (H.R. Bakhsheshi-Rad).

